β-Amyloid accumulation in the human brain after one night of sleep deprivation

Ehsan Shokri-Kojori[a,1], Gene-Jack Wang[a,1], Corinde E. Wiers[a], Sukru B. Demiral[a], Min Guo[a], Sung Won Kim[a], Elsa Lindgren[a], Veronica Ramirez[a], Amna Zehra[a], Clara Freeman[a], Gregg Miller[a], Peter Manza[a], Tansha Srivastava[a], Susan De Santi[b], Dardo Tomasi[a], Helene Benveniste[c], and Nora D. Volkow[a,1]

[a]Laboratory of Neuroimaging, National Institute on Alcohol Abuse and Alcoholism, National Institutes of Health, Bethesda, MD 20892; [b]Piramal Pharma Inc., Boston, MA 02108; and [c]Department of Anesthesiology, Yale School of Medicine, New Haven, CT 06510

The effects of acute sleep deprivation on β-amyloid (Aβ) clearance in the human brain have not been documented. Here we used PET and ^{18}F-florbetaben to measure brain Aβ burden (ABB) in 20 healthy controls tested after a night of rested sleep (baseline) and after a night of sleep deprivation. We show that one night of sleep deprivation, relative to baseline, resulted in a significant increase in Aβ burden in the right hippocampus and thalamus. These increases were associated with mood worsening following sleep deprivation, but were not related to the genetic risk (APOE genotype) for Alzheimer's disease. Additionally, baseline ABB in a range of subcortical regions and the precuneus was inversely associated with reported night sleep hours. APOE genotyping was also linked to subcortical ABB, suggesting that different Alzheimer's disease risk factors might independently affect ABB in nearby brain regions. In summary, our findings show adverse effects of one-night sleep deprivation on brain ABB and expand on prior findings of higher Aβ accumulation with chronic less sleep.

beta amyloid | sleep | hippocampus | Alzheimer's disease | glymphatic system

Beta-amyloid (Aβ) is present in the brain's interstitial fluid (ISF) and is considered a metabolic "waste product" (1). Mechanisms by which Aβ is cleared from the brain are not completely understood (2), although there is evidence that sleep plays an important role in Aβ clearance (3). In rodents, chronic sleep restriction led to increases in ISF Aβ levels (4) and in a *Drosophila* model of Alzheimer's disease (AD), chronic sleep deprivation (SD) resulted in higher Aβ accumulation (5). In healthy humans, imaging studies have revealed associations between self-reports of less sleep duration or poor sleep quality and higher Aβ burden (ABB) in the brain (6–8), which is a risk factor for AD. This association has been considered bidirectional because increased ABB could also lead to impairments in sleep (9, 10). Notably, increased ABB in the brain has been associated with impairment of brain function (11, 12). Thus, strategies that prevent Aβ accumulation in the brain could promote healthy brain aging and be useful in preventing AD. In this respect, there is increasing evidence that sleep disturbances might contribute to AD, in part by facilitating accumulation of Aβ in the brain (13).

To better characterize ABB dynamics, studies have focused on the effects of sleep patterns on ABB in the CNS. In rodents, it has been shown that Aβ clearance from the brain's ISF predominately occurred during sleep (4), which was ascribed to the glymphatic pathway, operating most efficiently during sleep (3, 14, 15). Clinical studies have also shown that Aβ levels in the cerebrospinal fluid (CSF) are the highest before sleep and the lowest after wakening, while CSF Aβ clearance was counteracted by SD (16). However, there are some inconsistencies between animal models and findings in humans (17), and Aβ increases in human CSF could reflect factors other than ABB increases in the brain itself (18–21). Notably, the effects of acute SD on Aβ clearance in the human brain have not been documented. This observation will be important for understanding the contribution of sleep to Aβ clearance from the brain and the regional specificity of such effects.

Here we evaluated the effects of one-night SD on ABB in healthy controls to investigate whether sleep affects clearance of Aβ from the human brain. For this purpose, we used positron emission tomography (PET) with which it is now possible to measure ABB in the living human brain. There are several validated PET radiotracers for this purpose, including ^{18}F-florbetaben (FBB) (22, 23). It is believed that such radiotracers predominantly bind to insoluble $A\beta_{42}$ plaques (24–27), but there is recent evidence that they also bind to soluble $A\beta_{42}$ forms (28). Thus, we reasoned that PET and FBB could be used to detect increases in ABB because of acute SD, directly in the human brain (3). First, we aimed to assess the effect of one-night SD on brain ABB with PET-FBB in healthy controls (n = 20, 22–72 y old, 10 females) (Table S1), and compared the measures to baseline brain ABB captured at the same time of the day but following a night of rested sleep [referred to as rested-wakefulness (RW)]. Second, we aimed to replicate in our sample the previously reported association between sleep history and brain ABB (when measured after RW) (6–8). For our first aim, we hypothesized that one night of SD would increase ABB in the hippocampus, which shows some of the earliest structural and functional changes in AD (29, 30). For our second aim, we hypothesized that history of poor sleep would be associated with

Significance

There has been an emerging interest in sleep and its association with β-amyloid burden as a risk factor for Alzheimer's disease. Despite the evidence that acute sleep deprivation elevates β-amyloid levels in mouse interstitial fluid and in human cerebrospinal fluid, not much is known about the impact of sleep deprivation on β-amyloid burden in the human brain. Using positron emission tomography, here we show that acute sleep deprivation impacts β-amyloid burden in brain regions that have been implicated in Alzheimer's disease. Our observations provide preliminary evidence for the negative effect of sleep deprivation on β-amyloid burden in the human brain.

higher ABB in the hippocampus, precuneus, and medial pre-frontal cortex (6, 8, 31).

Results

Acute SD Effects. To compare the differences in FBB binding [quantified as relative standard uptake value (SUVr) and used as a marker of ABB] (*Methods*) after acute SD versus that obtained after RW, we used a voxelwise paired *t* test in statistical parametric mapping (SPM) (*Methods*). This analysis showed that images obtained after SD compared with those obtained after RW had significantly higher FBB binding (ABB increases) in a right lateralized cluster (Fig. 1*A*) that comprised hippocampal, parahippocampal, and thalamic regions (Table S2). Of note, the increases in FBB SUVr in this cluster were robust and observed in 19 of 20 participants (Fig. 1*B*) from RW (mean = 1.35, standard deviation = 0.06) to SD (mean = 1.42, standard deviation = 0.07; a 5% increase, $P < 0.0001$). To further confirm this finding, we quantified FBB SUVr in an a priori hippocampal region of interest (ROI) (*Methods* and Fig. 1*D*) and compared the measures after SD to those after RW. This ROI analysis also showed a significant increase in FBB SUVr in the right hippocampus ROI from RW to SD ($P = 0.046$, two-tailed, Cohen's $d = 0.48$) but not in the left hippocampus ($P = 0.4$). The magnitude of the Aβ changes in the hippocampal cluster varied significantly between subjects (Fig. 1*B*) (−0.58% to +16.1%). We found that this variability was not associated with gender, age, or apolipoprotein E (APOE)-based odds ratio for AD (ORAD) (*Methods*) ($P > 0.3$). Notably, changes in FBB SUVr in the subcortical cluster were significant in both males ($P = 0.0008$) and females ($P = 0.003$). In addition, reported sleep hours (SH) and total score (TS) for sleep quality (Pittsburgh Sleep Questionnaire Inventory, PSQI) (*Methods*) were not associated with these SD-related increases. Thus, the mechanisms accounting for the observed between-subject variability are still unclear. Subjective behavioral assessment revealed that SD negatively impacted mood compared with RW (*Methods* and Fig. S1). We assessed if the effects of SD on mood were correlated with increases in ABB in the right hippocampal cluster. This analysis showed that mood worsening was negatively associated with changes in FBB SUVr [r (16) = −0.50, $P = 0.03$] (Fig. 1*C*) such that participants with larger increases in ABB in the hippocampal cluster (Fig. 1*A*) had more mood worsening after SD. Because the quantification of ABB using FBB SUVr can be sensitive to blood perfusion effects, we quantified FBB accumulation using measures of binding potential (BPnd), which are less sensitive to blood perfusion effects than SUVr measures. BPnd in the cluster where we observed the SD effect (*Methods* and Fig. 1*A*) was also significantly higher in SD relative to RW [$t(19) = 3.57, P = 0.002$] (Fig. S2*A*). Moreover, SD-related changes in BPnd were significantly correlated with those observed with FBB SUVr [$r(18) = 0.53, P = 0.016$] (Fig. S2*B*), further supporting that SD-related increases in FBB SUVr are not primarily driven by perfusion effects.

Sleep, APOE, and ABB. Prior studies had reported an association between reported SH and sleep quality and (cortical) ABB in healthy middle-aged and older individuals (6–8). We tested whether we would corroborate those observations in our sample using the measures obtained during RW. We found that reported average SH inversely correlated with FBB SUVr [$r(18) = −0.5$, $P = 0.024$] and with BPnd [$r(18) = −0.57, p = 0.009$] at RW in the subcortical cluster that showed increases in ABB with SD (Fig. 2*A*), thus supporting long-term susceptibility of these regions to increased ABB with less SH. Voxelwise regression analysis of FBB SUVr on SH showed that less SH was associated with higher FBB SUVr in the bilateral putamen, parahippocampus, and right precuneus (Fig. 2*B* and Table S3). Interestingly, the SH-related brain areas were more extensive than the areas associated with (acute) SD-induced ABB increases. For regional ABB, SH-related subcortical regions (Table S3) had minimal overlap with subcortical areas related to ORAD (Fig. 2*B*), which included the bilateral lentiform nucleus and pallidum (Table S4). These observations suggested that different brain
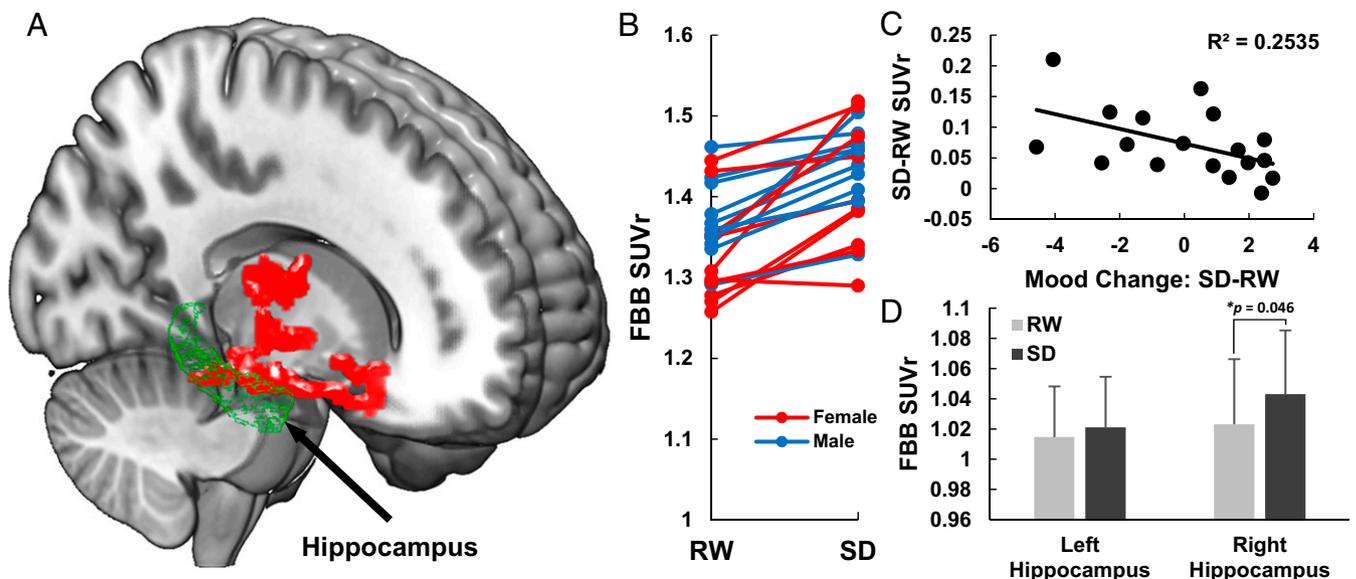

Fig. 1. Effects of one-night SD on ABB. (*A*) Voxelwise paired *t* test between RW and SD conditions highlighting the hippocampus as well as other subcortical structures ($P_{FWE} < 0.05$, cluster-size corrected) (Table S1). (*B*) Subject-level changes in FBB SUVr (in the red cluster identified in *A*) from RW to SD. There was no significant effect of gender, or gender × sleep interaction ($P > 0.15$). (*C*) Association between changes in mood from RW to SD and changes in the FBB SUVr for the cluster identified in *A*. Mood change was quantified using the principal component of the changes in self-report measures from RW to SD, which accounted for 35.5% of the variance. Self-report measures of alert, friendly, happy, social, and energetic significantly decreased, and measures of tired and difficulty staying awake significantly increased from RW to SD ($P < 0.001$, two-tailed) (see also Fig. S1). (*D*) Average FBB SUVr in a priori hippocampus ROIs across subjects. Error bars show standard deviation (*Methods*).
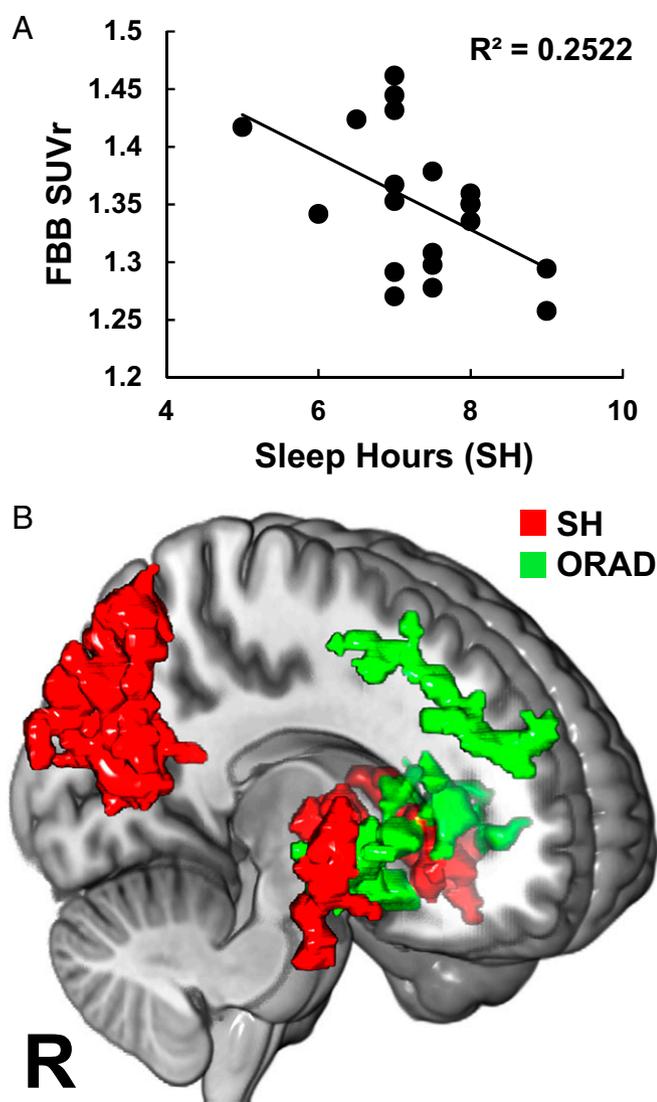
Fig. 2. Relationship between SH, APOE genotype, and ABB. (*A*) Regression of FBB SUVr (indexing ABB) for the red cluster shown in Fig. 1*A* at RW against SH. (*B*) Three-dimensional rendering of the areas showing an association between higher FBB SUVr at RW and lower SH (red clusters, P_{FWE} < 0.05, cluster-size corrected) (Table S3), as well as areas showing an association between higher FBB SUVr and higher APOE-based genetic risk for AD (quantified as log of ORAD) (green clusters, P_{FWE} < 0.05, cluster-size corrected, except the right-sided subcortical cluster, which was cluster size-corrected at q_{FDR} < 0.05) (Table S4). The subcortical clusters related to SH and ORAD had minimal spatial overlap (18 voxels, <3%) (Tables S3 and S4). Notably, FBB SUVr within the SH-related subcortical clusters (red, *B*) was not associated with ORAD (P = 0.25) and FBB SUVr within the ORAD-related subcortical clusters (green, *B*) was not associated with SH (P = 0.2).

regions could be independently affected by different AD-risk factors (i.e., sleep vs. APOE). This observation is consistent with prior findings reporting that the APOE genotype did not moderate the relationship between sleep measures and ABB in the brain (7).

Discussion

Our findings provide preliminary evidence for the role of SD on Aβ accumulation in the human brain. The increases in ABB after SD in the hippocampus, which is considered among the most-sensitive brain regions to AD neuropathology (29), is consistent with epidemiological data identifying impaired sleep as a risk

factor for AD (9, 10) and with recent evidence showing that disruption of deep sleep increases Aβ in human CSF (32). We also showed Aβ increases in the thalamus after SD, which is a brain region that shows increases in Aβ in the early stages of AD (33). The regional increases in ABB that we observed from RW to SD might reflect decreased clearance of Aβ, presumably from lack of sleep, thus supporting the role of glymphatic system in clearing Aβ from the brain during sleep. While this effect was observed in rodents (3), no study as of now has been able to directly measure Aβ clearance reflecting glymphatic function in the human brain. Other mechanisms have been shown to stimulate Aβ clearance during sleep, such as γ-oscillations during the rapid eye-movement cycle (34). Alternatively, Aβ increases in the hippocampus after SD could reflect increases in Aβ synthesis associated with endogenous neuronal activity during SD (35), or sleep-related changes in hippocampal neurogenesis (36, 37). While we are interpreting our findings of increases in ABB after SD to reflect Aβ accumulation due to lack of glymphatic clearance (or other unknown mechanisms), we cannot rule out the possibility that they reflect increases in the synthesis of Aβ (38) from lack of sleep. Preclinical studies that monitor Aβ clearance during sleep using PET radiotracers alongside optical imaging of ISF are needed to corroborate whether Aβ ligands and PET have potential as markers of glymphatic function in the human brain. Future work should also study the extent that elevated ABB in the brain is related to increases in Aβ levels in the peripheral tissue following SD (18, 20).

Detection of Aβ plaques with PET is clinically relevant for the diagnosis of AD, while elevated brain ABB in mild cognitive impairment (MCI) has been suggested as a risk factor for progression to AD (22, 39). ABB increases as a function of aging and AD severity, with an estimated 17% increase from younger to older adults (40). Relative to healthy elderly, estimated increases of 21% and 43% have been reported in individuals with MCI and AD, respectively (40). In our study, the increases in ABB due to one-night SD were smaller (5%) (Fig. 1 *A* and *B*) and were observed in a subcortical cluster that included the hippocampus. At this stage, we are uncertain whether such SD-related increases in ABB may subside following rested sleep. In addition, the magnitude of the observed effects should be interpreted with caution considering the methodological limitations and potential confounds, such as the effects of blood-flow changes and the limited sensitivity of current PET radiotracer to soluble Aβ (28). While, prior studies have reported associations with chronic poor sleep and higher average ABB across large a priori-selected cortical areas (6–8), our results highlight the relevance of studying subcortical regions for the associations between ABB and sleep.

It has been shown in rodents that Aβ plaques can form very rapidly (41), while Aβ plaques in their earliest stages show the highest levels of neuritic dystrophy (42), thus suggesting that increases in ABB due to one-night SD could adversely impact the brain. Chronic poor sleep could then result in higher baseline ABB levels, helping to explain the association with higher ABB at RW (in the cluster showing SD effects) (Fig. 1*A*) and less reported SH (Fig. 2*A*). In addition, SH negatively correlated with ABB in the precuneus, putamen, and parahippocampus (Fig. 2*B* and Table S3). These findings are consistent with studies showing that chronic sleep restriction lead to elevated cortical Aβ oligomers levels (that are neurotoxic) in the mouse cortex (43), which might in part reflect up-regulation of β-secretase 1 (44). However, a confounder is that increased ABB could in turn exacerbate sleep problems (10).

It is noteworthy that ABB increases in the hippocampus are less pronounced in MCI (45) or early-stage AD than in the precuneus (22). Instead, changes in hippocampal volume, glucose metabolism (30), and the blood–brain barrier (46) were most evident in patients with early-stage AD. Thus, it is possible

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that the increases in ABB in the hippocampus with sleep disruptions might trigger local neurotoxicity without necessarily resulting in marked plaque accumulation. The precuneus was not significantly affected by SD; however, we found an association between reported SH and ABB in this region (Fig. 2B and Table S3), again suggesting that distinct processes might mediate the effects of acute vs. chronic SD on regional ABB. Future work should investigate the extent to which the effects of acute SD and less SH might reflect distinct mechanisms (i.e., neuroinflammation triggered by chronic poor sleep) (47, 48) or sensitivity of FBB to different forms of Aβ (soluble oligomers vs. plaques) (28). One limitation of this work includes the inability of PET-FBB to distinguish soluble from insoluble Aβ (27, 28, 49). We suggested that the interruption of glymphatic clearance by SD would increase ABB in the brain, yet our findings do not demonstrate the mechanisms that account for the Aβ accumulation with SD. In our study, estimates of ABB were obtained using FBB SUVr, which is sensitive to physiological factors such as blood flow, which could have been impacted by SD (50, 51). However, recent evidence suggests that blood-flow effects are small on FBB SUVr estimated with later time points (52) (*Methods*). We also corroborated the FBB SUVr findings with BPnd measures that are less sensitive to blood-flow effects (Fig. S2).

In our study, we did not predict the laterality effect for the SD-related increases in ABB, and while this could reflect the sensitivity of the glymphatic system to orientation of the head during sleep (14), we did not record head position. Consistent with the recognized role of the hippocampus and thalamus in mood disorders (53), the association between SD-related increases in ABB and mood worsening (Fig. 1C) supported the functional significance of elevated ABB. This association could reflect the previously reported contribution of the hippocampus in modulating mood changes that follow SD (54). The effects of SD on the hippocampus have also been implicated in the memory impairment associated with SD, although we did not measure effects of SD on memory in our study. Even though our sample was small ($n = 20$), we were able to identify a significant effect of SD on brain ABB with no significant interaction with gender. Because of the small sample size of our study, future studies are needed to assess the generalizability to a larger and more diverse population and to more reliably characterize potential gender effects.

In summary, this study documents an effect of one-night SD on ABB in the hippocampus, thus providing preliminary evidence that sleep, among other factors, could influence Aβ clearance in the human brain. Our results highlight the relevance of good sleep hygiene for proper brain function and as a potential target for prevention of AD (31, 55).

Methods

Participants. Twenty-two healthy individuals were recruited at the National Institutes of Health, of which 20 (10 females, age: 39.8 y ± 10.4, range: 22–72 y old) completed two PET scan sessions to measure ABB. All participants provided informed consent to participate in the study that was approved by the Institutional Review Board at the NIH (Combined Neurosciences White Panel). Exclusion criteria were: (*i*) urine positive for psychotropic drugs; (*ii*) history of alcohol or drug use disorders; (*iii*) present or past history of neurological or psychiatric disorder, including evidence of cognitive impairment; (*iv*) use of psychoactive medications in the past month (i.e., opiate analgesics, stimulants, sedatives); (*v*) currently taking prescription medications (i.e., antihistamines, antihypertensive, antibiotics); (*vi*) medical conditions that may alter cerebral function; (*vii*) cardiovascular and metabolic diseases; and (*viii*) history of head trauma with loss of consciousness longer than 30 min. Table S1 summarizes physiological and neuropsychological assessment to ensure participants were healthy and were not cognitively impaired.

Structural MRI. Participants also underwent MRI in a 3.0 T Magnetom Prisma scanner (Siemens Medical Solutions) using a 32-channel head coil to collect T1-weighted 3D MPRAGE (TR/TE = 2,400/2.24 ms, 0.8-mm isotropic resolution) and T2-weighted spin-echo multislice (TR/TE = 3,200/564 ms, 0.8-mm in-plane resolution). MRI was processed using the minimal preprocessing pipeline of the Human Connectome Project (56). Specifically, FreeSurfer v5.3 (Martinos Center for Biomedical Imaging; https://surfer.nmr.mgh.harvard.edu/) was used for anatomical data segmentation. In addition, each MRI image underwent gradient distortion correction, field map processing, spatial normalization to the stereotactic space of the Montreal Neurological Institute (MNI) with 2-mm isotropic resolution, and brain masking using routines from University of Oxford's Center for Functional Magnetic Resonance Imaging of the Brain Software Library release 5.0 (https://fsl.fmrib.ox.ac.uk/fsl/fslwiki). FreeSurfer segmentation ('wmparc.nii') in the MNI space was used for generating a subject-specific mask of the hippocampus (label numbers: 17 and 53 for left and right hippocampus, respectively).

PET Data Acquisition. The PET scans were performed using a high-resolution research tomography Siemens scanner on two separate scan days with FBB. FBB was injected through an intravenous catheter in about 1 min using a Harvard pump. Dynamic scanning started immediately after FBB injection, with 1.23-mm isotropic resolution using list-mode acquisition. During the PET imaging procedures, the participants rested quietly under dim illumination. To ensure that subjects did not fall asleep, they were monitored throughout the procedure and asked to keep their eyes open (no fixation cross). Information about head movement was collected using a cap with small light reflectors and a Polaris Vicra (Northern Digital) head-tracking system to minimize motion-related image blurring. Before FBB injection, a transmission scan was obtained using cesium-137 to correct for attenuation.

FBB-PET Scans. Each participant underwent two FBB-PET scans to measure ABB, one scan on a day following RW and another scan on a day following a night of SD. For this purpose, participants stayed overnight at the Clinical Center at the NIH before their scheduled SD or RW scans. For the SD condition, participants were instructed to wake up at 8:00 AM on the morning before the SD night. Upon arrival, participants were continuously accompanied by a nurse to ensure that they stayed awake for the SD condition during their stay. For the RW conditions, nurses observed whether patients were asleep every hour from 10:00 PM to 7:00 AM. On the day of RW, the participants were woken up at 7:00 AM. On both days, participants remained under supervision of the nurse and were brought to the PET imaging center before the scan, which started around 1:30 PM. Thus, participants remained awake for a total of about 31 h (including the scan length) during the SD condition. No food was given after midnight and caffeinated beverages were discontinued 24 h before the study. Patients had a light breakfast and lunch on the scan day. The order of RW and SD scans was counterbalanced across subjects and were, on average, 15 d apart (standard deviation = 19 d). In preparation for the scans, a catheter was placed for radiotracer injection. Dynamic scanning started right after intravenous injection of about 9.5 mCi (or less) of FBB, which lasted for 120 min. During FBB scans, participants were encouraged to listen to music to stay awake.

PET Data Analysis. FBB uptake in the brain was quantified using the SUVr using the whole cerebellum as reference region for images obtained from later time points (90–110 min) (57, 58). We chose the SUVr method given the recent evidence (for a radiotracer from the same family as FBB) that the SUVr approach of estimating tracer accumulation, relative to other noninvasive kinetic modeling approaches, had one of the highest correlations, with arterial input compartment modeling results ($R^2 = 0.95$), and had comparable accuracy, while maintaining much simpler modeling requirements and not suffering from voxel-level noise on model fitting (59). Despite the concern that SUVr estimates of radiotracer accumulation are affected by confounds such as blood-flow changes, recent work has suggested a limited influence of blood-flow changes on FBB SUVr measures obtained from the later time points, similar to the range used in our study (i.e., 90–110 min) (52). SUVr images for FBB were coregistered with individual subjects' T1-weighted images and resampled into 2-mm isotropic resolution before being transformed into the MNI space using the same normalization parameters that were generated for T1-weighted (and T2-weighted) images. For statistical parametric mapping, images were smoothed with a 4-mm kernel and masked at 0.5 SUVr to remove voxels outside the brain. We also performed a follow-up BPnd analysis to address the concern that FBB SUVr might have been affected by confounds, such as changes in blood flow and tracer clearance properties (52, 60). Specifically, regional BPnd was

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calculated using a noninvasive simplified reference tissue model (SRTM) (61, 62) that was fitted to the time activity curve (0–120 min) derived from the subcortical cluster showing a significant effect of SD on FBB SUVr (Fig. 1A). We also corroborated SRTM-based BPnd findings using the reference Logan approach (Fig. S2) (59, 63). Kinetic modeling of dynamic PET data was performed in the PMOD Kinetic Modeling Tool v3.605 (PMOD Technologies). For consistency with the SUVr approach, the whole cerebellum was used as the reference region for the BPnd analyses.

Pittsburgh Sleep Quality Index. The PSQI questionnaire (64) was administered to all participants ($n = 20$). For the analyses, we used the number of SH and the TS quality score from the PSQI, because prior studies have linked these sleep measures to brain ABB (6, 65, 66). While SH is a self-report of participants' SH at night (excluding times spent awake in bed), TS is a composite of scores of sleep quality, latency, hours, efficiency, medication, disturbances because of one's health or sleep partners, and daytime life quality (lower TS indicates better sleep quality).

APOE Genotyping. SNPs of the APOE gene (rs7412 and rs429358) have been shown to influence brain glucose metabolism and ABB (67, 68). Accordingly, in all participants we genotyped rs7412 and rs429358 SNPs of APOE and computed a log of ORAD for each participant, following the methods of a previous study (69), normalized relative to the population risk for AD. We used ORAD to evaluate whether APOE influenced the association between sleep and ABB.

Mood Questionnaires. Mood questionnaires were collected periodically (five times) throughout the RW and SD scans in 18 of the 20 participants. Questionnaires were acquired at least an hour apart, prior (three measures), during (one measure), and after (one measure) the PET scans. On a scale of 0–10, subjects rated whether they felt alert, tired, hungry, friendly, happy, sad, anxious, irritable, social, confused, bored, comfortable, energetic, caffeine craving, and difficulty staying awake. The scores across the five time-points

were averaged for each mood measure for each scan day. The first principle component of the standardized SD–RW difference scores for the 15 self-report mood measures was computed to summarize the change in mood from RW to SD into one component. This component accounted for 35.5% of the variance of the mood change measures (SD–RW) and was positively correlated with changes in ratings of feeling alert, friendly, happy, social, and energetic ($P < 0.01$, two-tailed), and negatively correlated with changes in ratings of feeling tired, anxious, and irritable from RW to SD ($P < 0.01$, two-tailed). Higher scores along this component reflected positive changes in mood from RW to SD.

Statistical Parametric Mapping. SPM8 (Wellcome Trust Centre for Neuroimaging) (70) was used for performing a voxelwise paired t test between SD and RW in FBB SUVr and voxelwise correlation between behavioral or genotyping measures and PET data. All effects were thresholded at $P \leq 0.015$ in SPM8 and a minimum cluster size of 300 voxels (2-mm isotropic). We chose this threshold based on the low sensitivity of FBB to soluble Aβ (28), but effects were corrected for multiple comparisons for cluster size using the random field theory (71) (family-wise error, FWE), or unless indicated, with false-discovery rate (FDR) in SPM8.

Data Availability. Subject-level measures used in the manuscript are available in Dataset S1. Please contact corresponding authors for additional information.

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