

# Supporting Information

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## SI Materials and Methods

**Human Subjects. Retinal cross-sectional imaging and analysis.** Optical coherence tomography (OCT) scans were obtained with a spectral domain (SD) system (RTVue-100; Optovue). The Line or HD-Line protocols were used to obtain 4.5- or 9-mm-long overlapping scans along vertical meridian crossing the fovea and extending up to 9-mm eccentricity (1, 2). Postacquisition processing of data was performed with custom programs (MatLab 7.5; MathWorks). OCT scans were aligned by the major retinal pigment epithelium (RPE) reflection in each longitudinal reflectivity profile (LRP), registered, merged, and resampled at 512 LRPs per 4.5 mm. Outer photoreceptor nuclear layer (ONL) was segmented manually using a combination of intensity and local slope information of LRPs (2, 3). Specifically, the hyporeflexive layer corresponding to the ONL (and the Henle fiber layer) was detected by placing the boundaries at the minimum LRP slope immediately distal (sclerad) to the hyperreflective outer plexiform layer (OPL) and maximum LRP slope proximal (vitread) to the hyperreflective outer limiting membrane (OLM) layer. The ONL was usually first defined in centrally retained regions and extended laterally to more peripheral regions with thinner ONL. Some data from the earliest visit in a subset of patients were acquired on a time-domain system (OCT3; Carl Zeiss Meditec) and analyzed as previously described (4–6).

Because normal ONL thickness changes with eccentricity, a parameter named ONL fraction was derived by dividing ONL thickness measured at each location by the mean normal ONL thickness at the corresponding retinal location (7). ONL fraction values were averaged across 1.2-mm spans between 1.2- and 8.4-mm superior retina and 1.2- and 6-mm inferior retina to reduce noise. A model of disease progression consisting of a delayed exponential function was hypothesized to underlie the change of ONL fraction with age (2, 8). Serial data were obtained in patients in yearly (or longer) intervals, and the rates of exponential decay associated with each pair of sequential data were calculated. The median value of all of the progression rates was assumed to estimate, to a first approximation, the underlying invariant progression rate. Next, the onset of the photoreceptor degeneration was estimated by fitting (least squares on log-linear coordinates) the invariant rate to all data from each individual retinal location and calculating the age at which the function intercepts the unity ONL fraction. The overall variation expected along the natural history of photoreceptor degeneration across all untreated control eyes and all retinal locations was estimated as the 2 SD of the residuals between the data replotted as a function of time after the onset of degeneration and the underlying natural history model (Fig. 1*F*). Serial data from study eyes (both treated and untreated retinal locations) of *RPE65*-LCA were similarly processed to derive ONL fraction. Next, data from each retinal location were horizontally shifted to match the baseline values to the natural history of progression, and the posttreatment values were compared with the expected natural history of degeneration (Fig. 2*B*).

**Psychophysical studies.** Visual sensitivity of patients was determined with a modified computerized perimeter (Humphrey Field Analyzer; Zeiss) as published (7, 9). The achromatic (white) stimulus was 1.7° in diameter and 200 ms in duration (maximum luminance = 3,180 cd.m<sup>-2</sup>), and it was presented after patients' eyes were adapted to darkness for an extended (3–8 h) period (7). Tested loci were along the vertical meridian crossing fixation. In all patients, testing was performed in study and control eyes at baseline and posttreatment time points. In a subset of patients, there was additional data available ranging up to 4.5 y

before treatment, providing serial measurements for up to 6.7 y. Retinal loci were sampled at 0.6-mm intervals up to 9-mm eccentricity from the fixation. Loci were tested using a red fixation target with a variable intensity that was adjusted to be visible for each subject.

The dynamic range of the native instrument (normally 5 log<sub>10</sub> units) was shifted with the use of neutral density filters (up to 3 log<sub>10</sub> units) to circumvent ceiling effects that would be otherwise expected in normal subjects and treated regions of some of the patients. In treated eyes, multiple tests were performed with overlapping dynamic ranges; floor or ceiling values were discarded, and best sensitivities were used.

**Dogs. Retinal cross-sectional imaging and analysis.** *En face* and retinal cross-sectional imaging was performed with the dogs under general anesthesia (10, 11). Overlapping *en face* images of reflectivity with near-infrared (NIR) illumination (820 nm) were obtained (Spectralis) with 30°- and 55°-diameter lenses to delineate fundus features, such as optic nerve, retinal blood vessels, boundaries of injection blebs, retinotomy sites, and other local changes. Custom programs (MatLab 7.5; MathWorks) were used to digitally stitch individual photos into a retina-wide panorama. In a subset of eyes, short-wavelength (488 nm) illumination was used to delineate the boundary of the tapetum and pigmented RPE. SD-OCT was performed with linear and raster scans (RTVue-100 by Optovue or Spectralis HRA+OCT). Linear scans were placed across regions or features of interest, such as bleb boundaries, to obtain highly resolved local retinal structure. The bulk of the cross-sectional retinal information was obtained from overlapping raster scans (6 × 6 mm, 101 lines of 513 LRPs each, no averaging; Optovue; 9 × 6 mm, 49 lines of 1,536 LRPs each, averaging 8–10; Spectralis) covering large regions of the retina extending ~24 × 24 mm<sup>2</sup>.

Postacquisition processing of OCT data was performed with custom programs (MatLab 7.5; MathWorks). For retina-wide topographic analysis, integrated backscatter intensity (OCT projection image) of each raster scan was used to locate its precise location and orientation relative to retinal features visible on the retina-wide mosaic formed by NIR reflectance images. Individual LRPs forming all registered raster scans were allotted to regularly spaced bins (1° × 1°) in a rectangular coordinate system centered at the optic nerve; LRPs in each bin were aligned and averaged. Intraretinal peaks and boundaries corresponding to histologically definable layers were segmented semiautomatically with manual override using both intensity and slope information of backscatter signal along each LRP. Specifically, the retina-vitreous interface, OPL, OLM, signal peak near the inner/outer segment junction, and RPE were defined. In the superior retina of the dog, backscatter from the tapetum forms the highest intensity peak, and RPE and inner/outer segment peaks are located vitreal to the tapetal peak. ONL thickness was defined from the sclerad transition of the OPL to the OLM, and ONL thickness topography was calculated. For all topographic results, locations of blood vessels, optic nerve head, and bleb boundaries were overlaid for reference.

Normal ONL maps were registered by the locus of the optic nerve head and rotated to bring the superior central vessels in congruence. A map of mean normal ONL thickness was derived. *RPE65*-mutant dog ONL maps similarly were registered to the normal map, and an ONL fraction was derived by dividing each thickness by the corresponding mean normal value. This derived ONL fraction map was sampled at five locations: two loci were in

the superior retina, two loci were in the inferior retina, and one locus was in the central nasal retina near the visual streak (Fig. 3 A–C). Natural history of photoreceptor degeneration was estimated by plotting ONL fraction values at these loci against age. **Electroretinography.** Dogs were dark-adapted overnight, premedicated, and anesthetized as described (12–15). Pupils were dilated. Pulse rate, oxygen saturation, and temperature were monitored. Full-field electroretinograms (ERGs) were recorded with Burian–Allen (Hansen) contact lens electrodes and one of two different computer-based systems with similar flash stimuli. Dogs 23–27 (D23–D27) were tested with the EPIC-XL (LKC Technologies) equipment previously described (15). D16, D17, D19, and D22 were tested with an Espion (Diagnosys LLC) system. White flashes ( $0.4\text{--}1.2 \log \text{scot}\cdot\text{cd}\cdot\text{s}\cdot\text{m}^{-2}$ ) were presented under dark-adapted conditions or flickered at 29 Hz on a rod-desensitizing background ( $0.8 \log \text{cd}\cdot\text{m}^{-2}$ ). In some cases, high-energy flashes were used to evoke photoresponses.

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**Morphological evaluation.** Assessment of photoreceptor structure was made in 6- to 7- $\mu\text{m}$ -thick retinal sections stained with H&E from eyes that were fixed in Bouin or Excalibur solution as previously described (16, 17). Using the *en face* retinal images and ONL topography maps as guides, eyes were trimmed to section through the treated and untreated regions. To correlate the degree of structural preservation with RPE65 expression, immunolabeling of adjacent sections was done with and without antigen retrieval using a polyclonal anti-RPE65 antibody (RPE65 PETLET; a gift from T. M. Redmond, Laboratory of Retinal Cell and Molecular Biology, National Eye Institute, National Institutes of Health, Bethesda) combined, when appropriate, with monoclonal antirhodopsin antibody (MAB5316; Millipore) using methods previously described (17). As control, we used retinal sections processed in the same manner from dogs that were WT or homozygous mutants at the RPE65 locus.









